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# Evanescent-Wave Cavity Enhanced Spectroscopy as a Tool in Label-Free Biosensing

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**Abstract:** A variety of evanescent-wave cavity-enhanced techniques is used in studying interfacial kinetics as well as the performance of anti-biofouling coatings, demonstrating the potential of these techniques in label-free biosensing.

OCIS codes: (300.1030) Absorption; (120.4820) Optical systems

### **1. Introduction**

Because of its simplicity and universality, UV absorbance detection is a generic detection method in liquid-phase analytical chemistry. However, the sensitivity of direct optical absorption detection is inferior to that of zero-background techniques such as fluorescence detection. The sensitivity of absorption detection in the visible range can be enhanced dramatically when the sample is placed in an optically stable cavity; the increased sensitivity stems from the increased optical path-length.

Conventionally, Cavity ring-down spectroscopy is based upon the abrupt termination of the optical excitation of a stable optical cavity followed by the measurement of the exponential decay of the light circulating in the cavity [1]. The exponential decay time decreases when an absorber is introduced into cavity. The sensitivity of CRDS stems from the increased optical path-length through the sample and the insensitivity to light source instabilities.

Incorporation of a fused silica substrate in the cavity allows for evanescent-wave (EW) sensing: only the highly localized evanescent wave of a total internal reflection event at the fused silica interface is used for measurements. By functionalizing the substrate surface, EW-CRDS has the potential to be used as a platform for label-free biosensing, providing an alternative for surface plasmon resonance detection.

## 2. Applications of cavity-enhanced techniques

Protein adsorption to silica surfaces is a notorious problem in analytical separations, and much effort has been and still is being dedicated to the development and characterization of anti-biofouling coatings [2]. Evanescent-wave cavity ring-down spectroscopy (EW-CRDS) and capillary electrophoresis (CE) were employed to investigate the capability of charged non-covalent coatings to minimize the adsorption of basic proteins. Conventionally, the performance of such coatings is quantified using separation parameters such as plate number, peak asymmetry and repeatability.

With EW-CRDS, the decrease of adsorption of cytochrome c to silica upon coating with a single and triple (sandwich) layers of polybrene and dextran sulfate could be directly quantified for the first time [3]. CE analyses of cyt c were performed with and without the respective coatings applied to the fused-silica capillary wall. Monitoring of the electroosmotic flow and protein peak areas indicated a strong reduction of irreversible protein adsorption by the positively charged coatings. Determination of the electrophoretic mobility and peak width of cyt c revealed reversible protein adsorption to the PB coating. The combination of results from EW-CRDS and CE provides highly useful information on the adsorptive characteristics of bare and coated silica surfaces toward basic proteins.

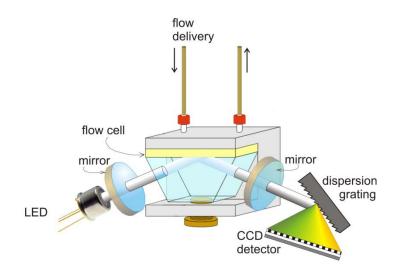


Fig. 1. Basic lay-out of an EW-CEAS system utilizing a LED as excitation source.

A novel broad-band mode of cavity-enhanced techniques is CEAS. A conventional absorbance spectrometer can be made into a CEAS setup simply by encompassing the sample in an optically stable cavity. A white light-emitting diode (LED) with emission between 420 and 700 nm and a supercontinuum (SC) source with emission between 450 and 2500 nm have been compared for use in evanescent wave broadband cavity-enhanced absorption spectroscopy (EW-BB-CEAS) [4]. The method is calibrated using a dye with known absorbance. While the LED is more economic as an excitation source, the SC source is superior both in terms of baseline noise (noise equivalent absorbances lower than  $10^{-5}$  compared to  $10^{-4}$  absorbance units) and accuracy of the measurement; these baseline noise levels are comparable to evanescent wave cavity ringdown spectroscopy (EW-CRDS) studies while the accessible spectral region of EW-BB-CEAS is much larger (420-750 nm in this study, compared to several tens of nanometres for EW-CRDS). The improvements afforded by the use of an SC source in combination with a high sensitivity detector are demonstrated in the broadband detection of electrogenerated Ir(IV) complexes in a thin-layer electrochemical cell arrangement. Excellent signal to noise is achieved with 10 ms signal accumulation times at a repetition rate of 600 Hz, easily fast enough to follow, in real time, solution kinetics and interfacial processes.

#### 3. Conclusion and future perspectives

The applicability of EW-CRDS in studying surface adsorption processes has been demonstrated by directly quantifying for the first time the amount of reversibly and irreversibly adsorbed protein on anti-biofouling coatings frequently used in CE.

Since CEAS is compatible with broad-band lightsources such as LEDs, CEAS is a promising route to costeffective and compact detectors of biomarkers. The performance of EW-CEAS using a super-continuum source and a LED as excitation source shows that the system utilizing an SC source gives superior detection performance but compromises the size and cost of the total system.

#### 4. References

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